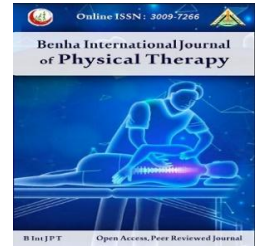


# Benha International Journal of Physical Therapy

Online ISSN: 3009-7266

Home page: <https://bijpt.journals.ekb.eg/>



Original research

## Influence of Induced Shoulder Complex Muscles Fatigue on Sensorimotor Functions of The Upper Extremity: A systematic review.

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### Article history:

Submitted: 01-03-2025

Revised: 16-03-2025

Accepted: 30-03-2025

### Abstract

**Background:** Induced fatigue of the shoulder muscles can significantly impact the kinematics and muscle power of the upper extremity, potentially leading to musculoskeletal injuries. Understanding these effects is crucial for developing effective interventions and rehabilitation protocols. **Purpose:** This systematic review investigated the impact of induced fatigue of the shoulder muscles on the sensorimotor functions of the upper extremity. **Methods:** The review followed PRISMA guidelines. A comprehensive search was conducted in five databases for clinical trials examining the effects of shoulder muscles fatigue on sensorimotor functions of the upper extremity. Inclusion criteria included various study designs. Data extraction covered participant characteristics, intervention details, outcome measures, and results. Data synthesis involved meta-analysis using MedCalc software. **Results:** A total of 25 clinical trials were included in this systematic review of which five studies went through meta-analysis. Induced fatigue significantly impacts the arthrokinematics of the glenohumeral joint, affecting the dispersion of the helical axis of rotation and altering the position of the humeral head within the glenoid cavity. Fatigue also alters humeral head migration. However, pooled statistical analysis of five studies showed no statistically significant difference in proprioceptive acuity ( $Z = 0.875$ , 95% CI  $[-1.037 - 2.708]$ ,  $P = 0.382$ ) with significant heterogeneity among the included studies ( $I^2 = 97.05\%$ ,  $P < 0.0001$ ). **Conclusion:** Induced fatigue of the shoulder complex musculature may influence the kinematics and muscle power of the upper extremity. However, the low methodological quality of the included trials and significant heterogeneity in the investigated variables hinder drawing definitive conclusions. More high-quality RCTs are required to reach a definitive conclusion regarding the effects of induced fatigue on upper extremity sensorimotor functions.

**Keywords:** induced fatigue; shoulder; kinematics; strength; proprioception.

## INTRODUCTION

Fatigue is one of the most common clinical problem that can be seen in both sports and work environment contributing to injury rate

and decrease the stability of the shoulder complex<sup>1</sup>. Muscle fatigue can be defined as the reduction in the highest amount of force or power that muscles can produce during

sustained activity<sup>2</sup>. Fatigue decrease muscle strength, affect shoulder range of motion and proprioception that could contribute to overuse injuries<sup>1</sup>.

The prevalence of fatigue worldwide was discussed in a recent systematic review including 91 studies with more than 623000 participants with a prevalence of 20.4% in adults which raise an alarm regarding this phenomenon that represents one of the top presented healthcare complaints in primary care settings<sup>3</sup>.

The shoulder complex consists of four articulations which are the glenohumeral joint, acromioclavicular joint, sternoclavicular joint and scapulothoracic joint which is not a true bony articulation<sup>4</sup>.

The articulations of the shoulder complex are mechanically linked and work in a coordinated manner to produce a specific kinematic that provides stability for the whole upper limb during functional tasks<sup>5</sup>. For instance, to reach full range of motion of the glenohumeral joint in the sagittal or frontal plane i.e., flexion or abduction, the scapula has to perform upward rotation, backward tilt and slight external rotation, additionally, the acromioclavicular joint rotates upward, the sternoclavicular joint retracts and rotates posteriorly, and the humerus rotates externally<sup>6</sup>.

These coordinated motions provide an optimal alignment of the scapular glenoid fossa with the head of the humerus playing an extensive and essential role in maintaining and providing stability in activities that demand a great deal of mobility of the shoulder joint in both sports activities such as volleyball, basketball, handball etc. and work environments such as carpentry, truck driving etc.<sup>7</sup>.

The muscular activity of the shoulder complex relies heavily on the afferent impulses reaching the central nervous system (CNS) from the variable sensory organs that exist in this area including the muscle spindles, the Golgi tendon organs and mechanoreceptors. These structures deliver sensory signals to the CNS such as the joint position sense, the forces applied to articular structures and tension

develop within the muscles, these data are integrated by the CNS to perform the desired movements efficiently<sup>8,9</sup>.

In shoulder complex, fatigue has an effect on normal shoulder kinematics including exacerbating scapular motions and decreasing shoulder elevation which may be attributed to delay in muscle activation, variation of muscle force production and reduced accuracy of the proprioceptive input<sup>10</sup>.

The effect of fatigue on proprioception can influence the motor control ability of the CNS on the shoulder complex's movement and jeopardize the joint stability and movement patterns<sup>11</sup>. Also, fatigue affects the neuromuscular pathways and alter motor unit firing, motoneuron excitability, and motor cortical excitability<sup>12</sup>. In addition, as muscles are the main stabilizers of the shoulder joint, fatigue could lead to disruption of the proximal stability of the shoulder joint leading to risks of shoulder instability<sup>13</sup>.

The current systematic review will discuss and investigate the impact of induced fatigue of the shoulder complex muscles to highlight its consequences such as shoulder complex and proximal shoulder instability and address them properly in order to reduce the possible risks of fatigue-related musculoskeletal injuries of the upper extremity.

## METHODS

This systematic review adhered to the Preferred Reporting Items of Systematic Reviews and Meta-analysis (PRISMA)<sup>14</sup>. The protocol was registered in PROSPERO database on 27<sup>th</sup> October 2024 (CRD42024602256).

### *Systematic Search*

PubMed, Web of Science, Scopus, Cochrane Central and Physiotherapy Evidence Database (PEDro) were searched for clinical trials investigating the impact of shoulder girdle muscles fatigue on sensorimotor functions of the upper extremity using the terms fatigue and shoulder in the title and abstract or title, abstract and keywords from inception till October 2024. The detailed search strategy is available in **Appendix (1)**.

The inclusion criteria included single group pre-test post-test studies, controlled trails, randomized controlled trails or crossover trails investigation the effect of induced fatigue of the shoulder complex musculature confirmed by valid objective or subjective measure on the sensorimotor functions of the upper extremity. Articles were excluded if they were not peer reviewed such as conference papers, theses or dissertation or articles written in any language other than English.

#### *Screening and Filtration*

Relevant records were imported into Mendeley software (Elsevier, Amsterdam, The Netherlands) and assessed against the predefined eligibility criteria through two phases; first through title and abstract then the remaining studies were assessed through their full text.

#### *Quality of Research and Risk of Bias Assessment*

Two independent authors used the PEDro scale to assess randomized controlled trails and controlled trails while methodological index for non-randomized studies (MINORS) scale will be used to assess non-comparative trails<sup>15, 16</sup>. The PEDro scale has 11 criteria of which only 10 are scored. The score of six is considered the cut-point at which the studies are considered of high quality i.e., 6-7 good and 8-10 excellent while studies scoring less than six is considered of low quality i.e., 4-5 fair and less than 4 is considered poor. The MINORS scale has eight items for non-comparative, each item has a maximum score of two with a total score of 16. Any discrepancy in the scoring was resolved by discussion with the senior author.

#### *Data extraction*

The following items were extracted from each included article and summarized in the data extraction sheet including the participants characteristics, the intervention characteristics, the outcome measures and the results.

#### *Data Synthesis*

The analysis started by calculating the arithmetic mean and standard deviation of paired difference between pre- and post-intervention values of each study. Then we calculated the standard error of the paired difference. The mean and the standard error of paired difference were used to calculate the pooled effect size across all included studies. Pooled effect size was expressed as the arithmetic mean and the 95%CI for every study as well as the weighted mean and the 95%CI across all studies. Heterogeneity across the studies was represented by  $I^2$  statistics. Fixed effect model was used as a default however, If heterogeneity was considerable ( $I^2 > 50\%$ ), the random effect model was used instead. 2-sided p value < 0.05 was considered statistically significant. Meta-analysis was done using MedCalc Version 23.0.2 for Microsoft Windows (MedCalc Software Ltd, Mariakerke, Belgium).

## **RESULTS**

The systematic search resulted in 563 records, after removal of duplicates using Mendeley software 273 records were included in the filtration process yielding a total of 25 included studies<sup>17-40</sup> **Figure (1)**. The main reason for exclusion was the inappropriate assessment of fatigue presence which is a crucial element in the inclusion criteria **Appendix (2)**.

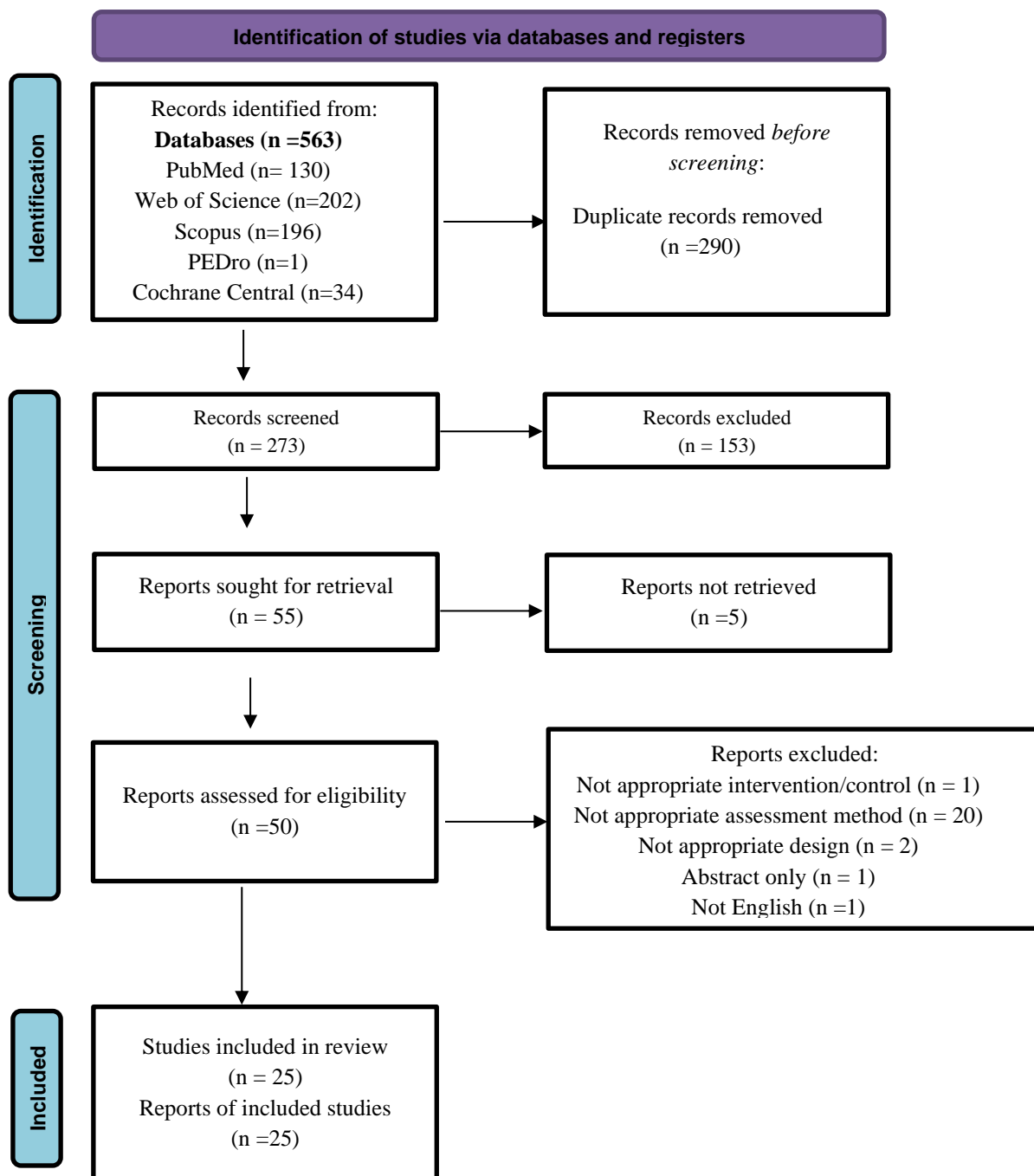


Figure (1): PRISMA flow diagram

Source: Page MJ, et al. BMJ 2021;372:n71. doi: 10.1136/bmj.n71.

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### Characteristics of the included studies

The included studies total population was 578 healthy participants across 25 studies. It is worth mentioning that seven studies included athletic participants<sup>24, 29, 31, 36, 38-40</sup>. The mean age of the participants included ranged from 20 to 35 years with 64% of the participant being males **Table (1)**.

Most of the included studies were single group repeated measure design without follow

up however, five studies were randomized crossover studies<sup>19, 24, 31, 32, 37</sup>, three studies were randomized controlled trails and one study was a controlled trail<sup>36</sup>. Their quality score ranged from 4 to 10 out of 16 for single group studies and 3 to 7 out of 10 for the controlled and RCTs **Table (2)**.

**Table (1): Characteristics of the included studies**

Study	Design	Population				Fatigue protocol	Outcome Measure	Results
		Type	N	Gender (M:F)	Age (Y)			
Adamo et al., 2020	SG pretest posttest	Healthy	30	NR	23.2±2.6	Isometric ex. At 50% of MVC for both shoulder flexors and ER until Borg score reached 10/10.	- Kinematics of shoulder joint (motion analysis)	- Following shoulder flexors fatigue of the dominant limb, significant increase was observed regarding mean distance, mean angle and decrease in ROM while ER fatigue significantly increased mean distance and mean angle only. - Regarding non-dominant limb, ER fatigue significantly increased mean distance and mean angle while flexors fatigue only affected mean angle and increased ROM.
Stella et al., 2024	SG pretest posttest	Swimmers	14	11:3	21±3	30 min of front-crawl swimming until Borg score reached 10/10	- TMG of PM, Trapezius and LD - Muscle power (HHD)	- TMG results showed statistically significant difference following fatigue protocol regarding LD and PM muscles only. - Only extension torque was affected following fatigue protocol.
Teyhen et al., 2008	SG pretest posttest	Healthy	20	20M	27.7±3.6	Rotator cuff fatigue through arm elevation in prone lying T- position with 5% of body mass until strength decreased by 40% from the prefatigue strength	- Muscle power (HHD) - GH migration (DFV)	- Significant differences were observed regarding GH migration and muscle strength following fatigue protocol.

Lida et al., 2014	Randomized crossover	Overhead athletes	15	15M	22.1±3.4	Isokinetic IR & ER fatigue protocol until the torque of ER decreased by 40% of the peak torque	<ul style="list-style-type: none"> <li>- JPS (isokinetic dynamometer)</li> <li>- ROM (motion analysis)</li> <li>- Muscle activity (EMG)</li> </ul>	<ul style="list-style-type: none"> <li>- IR and ER peak torque decreased significantly following IR and ER fatigue respectively while the opposite did not occur.</li> <li>- MPF of PM and LD decreased significantly following IR fatigue while infraspinatus decreased following ER fatigue.</li> <li>- IEMG of PM &amp; LD showed higher values following IR fatigue compared to prefatigued values also infraspinatus showed higher values following ER fatigue compared to prefatigued values.</li> </ul>
Joshi et al., 2011	SG pretest posttest	Overhead athletes	25	15:10	20±2	ER fatigue protocol using a dumbbell 25% of the baseline peak force generated by infraspinatus muscle until average ER peak force decreased by more than 25% from baseline peak force	<ul style="list-style-type: none"> <li>- Muscle activity (EMG)</li> <li>- Shoulder kinematics (motion analysis)</li> <li>- Muscle power (HHD)</li> </ul>	<ul style="list-style-type: none"> <li>- Regarding MVC, only the infraspinatus showed a significant decrease following fatigue protocol in the descending phase of the diagonal elevation pattern.</li> <li>- Scapular upward rotation was greater at post-fatigue compared to pre-fatigue, on contrast no differences were observed regarding anterior and posterior tilting or IR and ER.</li> <li>- Regarding EMG, RMS decreased significantly following fatigue in lower trapezius muscle only.</li> </ul>
Bowman et al., 2006	Randomized crossover	Overhead athletes	20	20M	24.76±4.03	Intervention: Bouts of baseball throwing from kneeling position until ball velocity decreased by 10% of the maximum recorded velocity. Control: No intervention for 20 min	- Deceleration time	- Significant difference was observed following fatigue protocol compared to control regarding shoulder deceleration time.



Henry et al., 2001	SG pretest posttest	Healthy	10	10M	20.2±3.6	Isokinetic fatigue protocol in functional diagonal pattern until the torque value fell below 25% of the initial peak-torque	- Muscle activity (EMG)	- No significant differences were observed regarding deltoid, infraspinatus and subscapularis muscles activity between pre-fatigue and post-fatigue assessment.
Guo et al., 2011	SG pretest posttest	Healthy	20	10:10	20±1.5	IR fatigue protocol using a dumbbell 80% of MVC until the measured maximum force was decreased to 50% below the initial maximum force	- Proprioceptive acuity (motion analysis)	- Fatigue of internal rotators did not affect the glenohumeral and scapulothoracic joints proprioception.
Carpenter et al., 1998	SG pretest posttest	Healthy	20	11:9	23.7±2.75	IR and ER isokinetic fatigue protocol until peak torque decreased by 50% of MVC	- Proprioceptive acuity (isokinetic dynamometer)	- Motion detection ability threshold significantly increased following fatigue protocol of both the IR and ER muscles

Ali et al., 2023	Randomized crossover	Overhead athletes	20	20 M	21.3±1.59	Prone kneeling & half kneeling ER fatigue protocol using dumbbell 70% of 1RM until Borg score reaches 15/20.	- Muscle power (HHD)	- Concentric contraction peak force, velocity, power, average power, and total work showed statistically significant difference in both groups compared to baseline measurements while eccentric contraction measurements were significant only in peak force, average power and total work. - No differences were observed between the two fatigue protocols.
Sterner et al., 1998	Randomized crossover	Recreationally active	20	20M	23.81±2.77	Isokinetic IR & ER fatigue protocol until peak torque declined below 50% of MVC.	- Proprioceptive acuity (isokinetic dynamometer)	- No significant differences were observed between fatigue and control groups regarding all proprioceptive acuity parameters.
Lee et al., 2003	SG pretest posttest	Healthy	11	11M	27.3±3	Isokinetic IR & ER fatigue protocol until peak torque declined below 50% of MVC.	- Proprioceptive acuity (isokinetic dynamometer)	- No significant difference between pre-fatigue and post-fatigue active and passive repositioning of IR and passive repositioning of ER however, active repositioning of ER revealed statistically significant difference compared to pre-fatigue condition.



Myers et al., 1999	RCT	Healthy active	32	16:16	21.82±1.46	Intervention: Isokinetic IR & ER fatigue protocol until peak torque declined below 50% of MVC. Control: No intervention for 5 min between assessment	<ul style="list-style-type: none"> <li>- Proprioceptive acuity (AAR)</li> <li>- Dynamic stability (SADS)</li> </ul>	- No statistically significant difference observed between groups regarding AAR test and SADS test.
Chang et al., 2006	SG pretest posttest	Healthy	13	5:8	24.46±2.07	Isokinetic IR & ER fatigue protocol until peak force declined below 50% of MVC	<ul style="list-style-type: none"> <li>- JPS (isokinetic dynamometer)</li> <li>- Muscle power (isokinetic dynamometer)</li> </ul>	- Muscle power decreased significantly following fatigue protocol by 39.75%
Voight et al., 1996	SG pretest posttest	Healthy	80	37:43	23.7±2.8	Isokinetic IR & ER fatigue protocol until declined below 50% of MVC	<ul style="list-style-type: none"> <li>- Proprioceptive acuity (Isokinetic dynamometer)</li> </ul>	Based on pre- and post-fatigue active and passive repositioning values, glenohumeral repositioning ability significantly changed following fatigue.

Côté et al., 2005	SG pretest posttest	Healthy	30	24:6	35±9.5	Continuous hammering at 70% of MVC till BORG scale reached a score of 8/10	<ul style="list-style-type: none"> <li>- UL kinematics (motion analysis)</li> <li>- Handgrip strength (handgrip dynamometer)</li> </ul>	<ul style="list-style-type: none"> <li>- Significant differences were observed regarding amplitude, peak velocity, peak acceleration and time interval regarding elbow movement and time interval in grip strength only.</li> <li>- Maximum grip strength decreased significantly following fatigue protocol compared to pre-fatigue condition.</li> </ul>
King et al., 2022	Controlled trial	Swimmers, WP players & healthy controls	37	37F	22.56±4	Isokinetic IR fatigue protocol until Borg score reached 8/10.	<ul style="list-style-type: none"> <li>- Muscle activity (EMG)</li> <li>- Muscle power (isokinetic dynamometer)</li> </ul>	<ul style="list-style-type: none"> <li>- Between group comparison statistical data were not reported.</li> </ul>
Dupuis et al., 2021	RCT	Healthy	40	24:16	26±3	<p>Intervention: Manipulating screws on a wooden board for two min, 20 rep of arm elevations in sagittal plane and 20 reps in scapular plane with 2 lb. dumbbell for women and 4 lb. for men until Borg score reached 8/10.</p> <p>Control: No intervention for 10 min break.</p>	<ul style="list-style-type: none"> <li>- Shoulder kinematics (IMUs)</li> <li>- Muscle activity (EMG)</li> </ul>	<ul style="list-style-type: none"> <li>- Anterior deltoid EMG amplitude showed a statistically significant increase favouring fatigue group in 40-60s measurement while MDF showed significant decreases in both 0-20s and 20-40s measurements. On contrast, Middle deltoid EMG results were similar between groups.</li> <li>- Joint kinematics during VR reaching tasks changed significantly following fatigue protocol compared to control with more reliance on trunk rotation and SC motion compared to GH motion.</li> </ul>

Thomas et al., 2023	SG pretest posttest	Baseball players	9	9M	20.1±1.1	Isokinetic ER fatigue protocol until peak force declined below 40% of MVC	<ul style="list-style-type: none"> <li>- Muscle activity (EMG)</li> <li>- Muscle synergies VAF (KINARM)</li> </ul>	- VAF changed significantly following fatigue in only one synergy out of four.
Dupuis et al., 2022	RCT	Healthy	40	24:16	26±3	<p><b>Intervention:</b> Manipulating screws on a wooden board for two min, 20 rep of arm elevations in sagittal plane and 20 reps in scapular plane with 2 lb. dumbbell for women and 4 lb. for men until Borg score reached 8/10.</p> <p><b>Control:</b> No intervention for 10 min break.</p>	<ul style="list-style-type: none"> <li>- Shoulder kinematics (IMUs)</li> <li>- Muscle activity (EMG)</li> </ul>	<ul style="list-style-type: none"> <li>- During the reaching tasks, SC elevation and spatiotemporal parameters of shoulder motion were statistically higher in the fatigue group compared to the control group.</li> <li>- EMG amplitude of upper trapezius showed statistically significant difference favouring the fatigue group compared to the control group.</li> </ul>
Sadler et al., 2019	Randomized crossover	Healthy	16	8:8	23.5±2.8	A repetitive pointing task performed to fatigue until Borg score reached 8/10.	<ul style="list-style-type: none"> <li>- Proprioceptive estimation task (KINARM)</li> </ul>	- Proprioceptive biases were less accurate in both the left and right hands.

Fuller et al., 2009	SG pretest posttest	Healthy	14	8:6	25.1±5.9	A repetitive reaching task to fatigue until Borg score reached 8/10.	- UL kinematics (motion analysis)	- The average shoulder joint position was located more superior in the SI direction, more towards the non-reaching side in the ML direction, and more posterior in the AP direction during fatigue. - The average elbow position was located significantly more posterior during fatigue while ML and SI average elbow positions were unaltered. Wrist joint linear ROM also increased in the AP direction.
Emery et al., 2012	SG pretest posttest	healthy	18	9:9	18-28	A repetitive pointing task performed to fatigue until Borg score reached 8/10.	- Proprioceptive acuity (motion analysis) - Muscle activity (EMG)	- No effect was observed of fatigue on Finger and shoulder position sense. - Muscle activity showed statistically significant increase following fatigue regarding anterior deltoid, middle deltoid and triceps.
Sutton et al., 2024	SG pretest posttest	Handball players	12	12M	26±4.6	Five bouts of 10 handball throwing tasks until Borg score reaches 15/20.	- JPS	- JPS was significantly affected following fatigue after bout one and five compared to the non-fatigued limb.

IRM: one repetition maximum; AAR: Active Angle reproduction; AP: Anteroposterior; DFV: Digital fluoroscopic video; Ex.: Exercises; GH: Glenohumeral; IMUs: Inertial measurement units; JPS: Joint position sense; LD: Latissimus dorsi; Min: minutes; ML: Medio-lateral; MVC: Maximum voluntary contraction; NA: Not applicable; NR: Not reported; PM: Pectoralis major; Reps: repetitions; RMS: Root mean square; SADS: single-arm dynamic stability; SC: Sternoclavicular; SG: single group; SI: superior-inferior; TMG: Tensiomyography; UL: Upper limb; VAF: Variance accounted for; VR: Virtual reality; Y: Years.

**Table (2): Characteristics of the included studies**

Single group studies (MINORS)									
Study	Q1: A clearly stated aim	Q2: Inclusion of consecutive patients	Q3: Prospective collection of data	Q4: Endpoints appropriate to the aim of the study	Q5: Unbiased assessment of the study endpoint	Q6: Follow-up period appropriate to the aim of the study	Q7: Loss to follow up less than 5%:	Prospective calculation of study size	Score (16)
Adamo et al., 2020	2	1	2	1	0	0	2	0	8
Stella et al., 2024	2	2	2	1	0	0	2	0	10
Teyhen et al., 2008	2	1	2	1	0	0	0	0	6
Joshi et al., 2011	2	1	2	1	0	0	0	0	6
Henry et al., 2001	2	1	2	1	0	0	0	0	6
Guo et al., 2011	2	1	0	1	0	0	0	0	4
Carpenter et al., 1998	2	1	2	1	0	0	0	0	6
Tse et al., 2016	2	1	2	1	0	0	0	0	6
Lee et al., 2003	2	1	2	1	0	0	0	0	6
Chang et al., 2006	2	1	0	1	0	2	0	0	6
Voight et al., 1996	2	1	1	1	0	0	0	0	5
Côté et al., 2005	2	1	2	1	0	0	0	0	6
Thomas et al., 2023	2	1	2	1	0	0	0	0	6
Fuller et al., 2009	2	1	2	0	0	0	2	0	7

Emery et al., 2012	2	1	2	0	0	0	0	0	0	0	5	
Sutton et al., 2024	2	1	2	1	0	0	2	0	8			
Comparative Studies (PEDro)												
	Q1: Eligibility Criteria	Q2: Randomization	Q3: Concealed Allocation	Q4: Baseline Similarity	Q5: Subjects Blinding	Q6: Therapists Blinding	Q7: Assessor Blinding	Q8: Drop-out	Q9: Intention-to-treat	Q10: between-group statistical comparisons	Q11: Measures of variability	Total (10)
Iida et al., 2014	No	1	0	0	0	0	0	0	0	1	1	3
Bowman et al.,2006	No	1	0	0	0	0	0	0	0	1	1	3
Sterne et al., 1998	Yes	1	0	1	0	0	0	0	0	1	1	4
Myers et al., 1999	No	1	0	1	0	0	0	0	0	1	1	4
King et al., 2022	Yes	0	0	0	0	0	0	1	0	1	1	3
Dupuis et al., 2021	Yes	1	0	1	0	0	0	1	0	1	1	5
Dupuis et al., 2022	Yes	1	0	0	0	0	0	1	0	1	1	4
Sadler et al., 2019	No	1	0	0	0	0	0	0	0	1	1	3
Ali et al., 2023	Yes	1	1	1	0	0	0	1	1	1	1	7



### Intervention Characteristics

Ten studies performed the fatigue procedure using isokinetic dynamometer fatigue protocol<sup>17-22, 25, 31, 36, 38</sup>, Five studies performed free weights active resistive exercises to fatigue<sup>26, 28, 29, 33, 37</sup> while the rest of the included studies induced fatigue throw performance of specific activities such as swimming<sup>39</sup>, baseball throwing<sup>24</sup>, handball throwing<sup>40</sup>, hammering<sup>23</sup>, combined manual activities<sup>34, 35</sup> and repetitive pointing or reaching tasks<sup>27, 30, 32</sup>. Fatigue was confirmed either throw decline in peak force and torque or rating of perceived exertion via Borg scale.

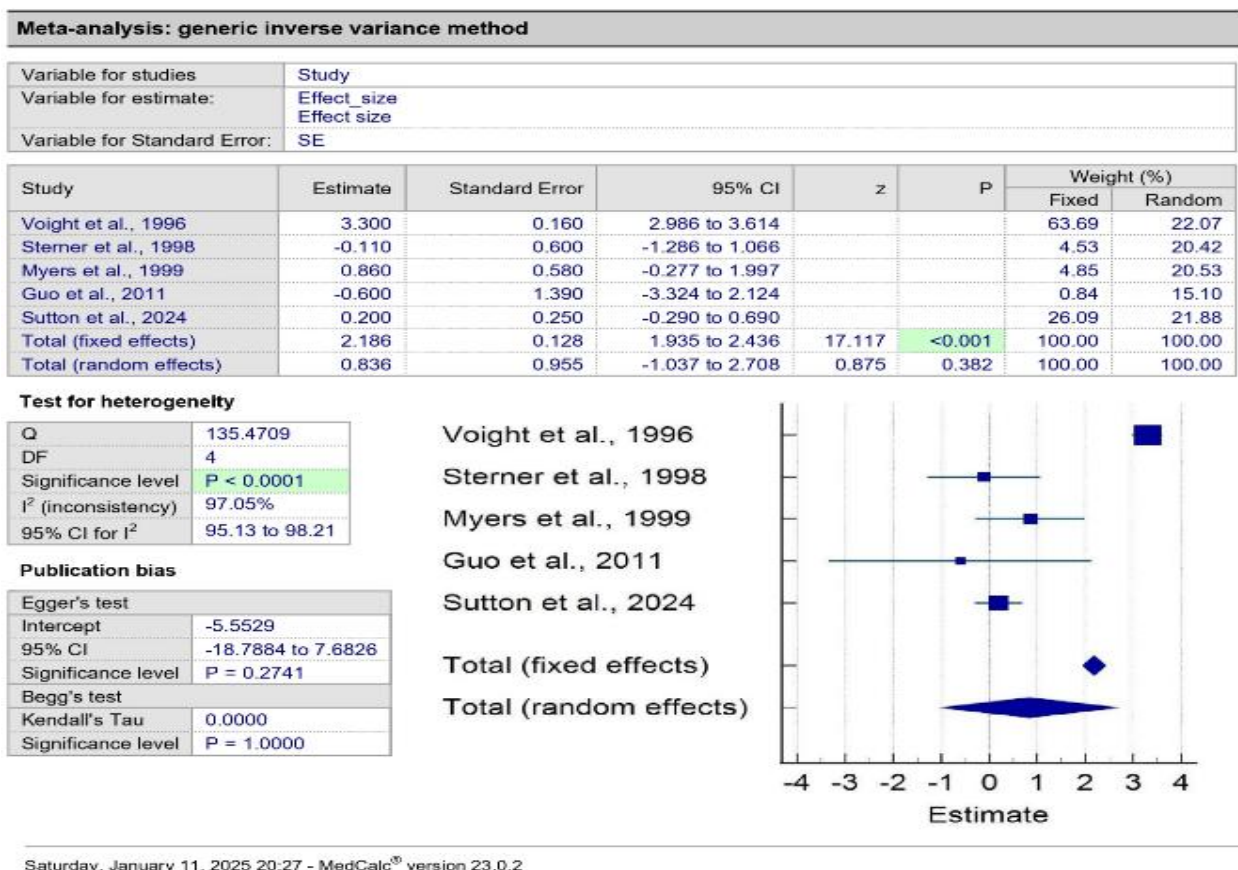
### Outcome measures

The main outcomes of interest were **proprioceptive acuity** via joint position sense or active reproduction test<sup>17-20, 22, 25, 28, 30-32, 40</sup>, **kinematics of upper extremity** including axes of rotation characteristics<sup>33</sup>, glenohumeral head migration<sup>26</sup>, range of motion<sup>27, 29, 31, 34, 35</sup>,

shoulder deceleration time<sup>24</sup>, spatiotemporal parameter of upper limb motion<sup>23</sup>, **muscle activity** mostly via electromyography<sup>21, 29-31, 34-36, 38</sup> or via tensiomyography<sup>39</sup> and **muscle power** either through hand held dynamometer or isokinetic dynamometer<sup>25, 26, 29, 36, 37, 39</sup> or handgrip dynamometer<sup>23</sup>.

### The effect of induced fatigue on proprioceptive acuity

Proprioceptive acuity was assessed via active reproduction of active and passive positioning tests, and threshold to detect motion tests. Five studies<sup>17, 19, 20, 28, 40</sup> were included in quantitative analysis showing no significant difference between fatigue and pre-fatigue condition ( $Z = 0.875$ , 95% CI [-1.037 - 2.708],  $P = 0.382$ ). It is worth mentioning that the data of the included studies showed significant statistical heterogeneity (97.05%,  $P < 0.0001$ ) so it was necessary to use the random effect model **Figure (2)**.



**Figure (2)** Descriptive Meta-analysis: Proprioceptive acuity pre & post fatigue comparison

*The effect of induced fatigue on kinematics of the upper extremity*

Kinematics of upper extremity was investigated in nine included studies<sup>23, 24, 26, 27,</sup>

<sup>29, 31, 33-35</sup>. The effect of induced fatigue was statistically significant in terms of dispersion of axis of rotation i.e., helical axis dispersion <sup>33</sup>, glenohumeral migration <sup>26</sup>, and shoulder joint angle and displacement <sup>27</sup>. Regarding, upper extremity range of motion, most of the included studies showed that fatigue statistically altered the ROM of upper extremity motions including scapular upward rotation, internal and external rotation, all GH motions, elbow flexion and extension <sup>23, 29, 33, 34</sup>, however scapular tilting <sup>29</sup> and glenohumeral abduction <sup>34</sup> did not show statistical differences following fatigue in two studies respectively.

The induction of fatigue in one shoulder affected also the contralateral shoulder specifically fatigue of shoulder flexor which resulted in higher ROM in the contralateral shoulder <sup>33</sup> and higher sternoclavicular elevation <sup>35</sup>, however, this did not affect the other joints in the contralateral limb and no effect was observed following external rotation fatigue protocol.

Post fatigue assessment of kinematics during the performance of sports or manual activities revealed increased deceleration time in baseball players <sup>24</sup> and decreased elbow velocity and acceleration during hammering <sup>23</sup>, however, it did not affect all other joints of during hammering task.

#### *The effect of induced fatigue on muscle power*

Muscle strength, power or torque were assessed in seven studies <sup>23, 25, 27, 31, 36, 37, 39</sup> via isokinetic dynamometer or handheld dynamometer. Single study <sup>23</sup> assessed handgrip strength via hand grip dynamometer. Most of the included studies revealed statistically significant decrease of muscle power following fatigue including shoulder extension, external rotation, internal rotation, shoulder elevation and handgrip strength <sup>23, 25, 27, 31, 36, 37, 39</sup>, however two studies showed insignificant results regarding shoulder flexion, internal and external rotation <sup>39</sup> and elbow flexion and extension <sup>27</sup>.

#### *The effect of induced fatigue on muscle activity*

Ten studies <sup>21, 27, 29-31, 34-36, 38, 39</sup> assessed muscle activity following fatigue. The assessed muscles were shoulder girdle muscles such as

trapezius, deltoid, pectoralis major, latissimus dorsi or rotator cuff muscles.

The muscle activity alteration varied across the assessed muscle; for instance, the upper trapezius activity increased following fatigue protocol in both the fatigued arm <sup>27</sup> and the contralateral arm <sup>35</sup> as well as the activity of pectoralis major muscle <sup>31, 36</sup>, however, it was not affected in overhead athletes <sup>29</sup>. On the contrary, the middle trapezius showed decreased activity in both healthy and water polo players <sup>36</sup> as well as the lower trapezius in overhead athletes <sup>29</sup>.

The results were conflicting regarding the activity of the anterior deltoid, middle deltoid, triceps, subscapularis, latissimus dorsi and infraspinatus muscles between the included studies <sup>21, 27, 30, 31, 34, 36</sup>, however, the activity of the posterior deltoid decreased following fatigue in both healthy controls and water polo players but not swimmers <sup>36</sup>. The serratus anterior and biceps brachii muscles were each studied in a single study revealing no difference between the prefatigue and post fatigue conditions <sup>27, 29</sup>.

Two studies used different assessment tools to assess muscle activity; One study <sup>39</sup> utilized tensiomyography to assess the activity of deltoid, latissimus dorsi, pectoralis major and the three parts of the trapezius muscles following 30 minutes of front-crawl swimming revealed significant difference in terms of maximal radial displacement in latissimus dorsi and pectoralis major and time of contraction of latissimus dorsi muscle while the other study <sup>38</sup> assessed the synergy of four groups of muscles revealing no difference following fatigue in all groups except the first group which included the middle trapezius, lower trapezius, middle deltoid, posterior deltoid and infraspinatus muscles.

## **DISCUSSION**

The current systematic review examined the effect of induced fatigue of the shoulder complex muscles on sensorimotor functions of the upper extremity in sedentary participants, active healthy participants and athletes. Considering the high risk of bias existing in the included studies and the significant

methodological and statistical heterogeneity, induced shoulder musculature fatigue may alter the joint kinematics and reduce the muscle power of the upper extremity, however, its effect on muscle activity and proprioception is questionable.

The results of the current systematic review showed that induced fatigue may have a clear impact on the arthrokinematics of the glenohumeral joint. The results of the included studies highlighted the effect of fatigue on dispersion of the helical axis of rotation of the glenohumeral joint which means that fatigue affected the position of the humeral head within the glenoid cavity <sup>33</sup>, in addition, another included study <sup>26</sup> which showed that fatigue altered humeral head migration.

This effect could be a risk factor to induce shoulder pathologies such as shoulder impingement syndrome as postulated in Yu et al., who reported that fatigue causes the humeral head superior migration in subjects with subacromial pain. This is due to weakness of rotator cuff muscles and overly active deltoid muscles, which result in changes to neuromuscular control and may lead to instability in the shoulder joint <sup>41</sup>. This is evident in Teyhen et al., that reported even in healthy participants, fatigue caused superior migration of the humeral head which could contribute to the incidence of shoulder impingement syndrome and rotator cuff pathologies <sup>26, 42</sup>

In addition, the induction of fatigue affected most of the range of motion parameters of the upper limb joints which may be attributed to the same mechanism as Cheng et al., stated that Loss of torque due to fatigue, decreased torque from muscle shortening, and passive tension in opposing muscles all lead to a reduced active range of motion <sup>43</sup>. This effect not only on the same extremity but rather extended to the contralateral extremity affecting the sternoclavicular and glenohumeral joints.

The impact of shoulder fatigue on the kinematics of the upper extremity was accompanied by its effect on muscle strength, power or torque. Most of the included studies reported reduction in muscle torque following

fatigue even though it extended to the handgrip strength, Fatigue decreases isometric force, slows maximum shortening velocity, and increases the curvature of the force-velocity relationship, all contributing to power loss <sup>44</sup>.

The effect of fatigue on muscle activity was ambiguous. The results were conflicting across many of the muscles investigated not only the presence of statistical significance of not but also, the direction of the effect was variable even in the same muscles i.e., increased or decreased activity. This highlights the issue of heterogeneity and variability of the methodological procedures adopted within the previous literature and not building upon the previous gained knowledge but rather adapting different methods without filling the existing gap within the current literature.

Even the only outcome that could be statistically pooled i.e., proprioception, although it showed no statistically significant effect of fatigue on proprioceptive acuity, the results come from the application of the random effects model of the meta-analysis which was obligatory due to the significant statistical heterogeneity (97.05%) within the included studies. This was confirmed by applying the fixed effects model and ignoring the statistical heterogeneity resulting in a very significant effect of fatigue on proprioception ( $P < 0.001$ ) however, it is not statistically appropriate.

### Limitations

The meta-analysis was only applicable in one outcome i.e., proprioception however, the statistical heterogeneity was very high i.e., 97.05%, also, the included studies showed high risk of bias and low methodological quality with great variability across the intervention procedures including the fatigue protocol which was applied through various activities and measurement procedures such as measuring different kinematic parameters and using different assessment tools. Furthermore, most of the included studies were single group repeated measure design and not randomized controlled trials which is a major defect, and the statistical designs and statistical data reported within the studies were inappropriate and inadequate. Also, this systematic review included only studies written in English,



however, most of the retrieved records were written in English.

### Future Implications

The results of this systematic review highlight the deficits in the methodological quality of this research point. There is an urgent need for well-structured randomized controlled trails with more standardized methods of induced fatigue, measurements and activities at which the outcome measures will be obtained. In addition, authors of clinical trials should shed light on the impact of fatigue on more types of athletic participants.

### CONCLUSION

Induced fatigue of the shoulder complex musculature may influence the kinematics and muscle power of the upper extremity. However, the low methodological quality of the included trials and significant heterogeneity in the investigated variables hinder drawing definitive conclusion regarding the effect of fatigue. More high quality RCTs are required to reach a definitive conclusion regarding the effects of induced fatigue on upper extremity sensorimotor functions.

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## Appendix I: Detailed search strategy

Database	Searching Strategy
PubMed	(Fatigue[Title] AND Shoulder[Title])
Cochrane Central	#1 ("fatigue":ti) #2 ("shoulder":ti) #1 AND #2
Web of Science	(TI=(fatigue)) AND TI=(shoulder)
Scopus	( TITLE ( fatigue ) AND TITLE ( shoulder ) )
PEDro	"Fatigue" "shoulder" Title only



## Appendix II: Details of Excluded Articles

Study	Exclusion Reason
Andrade et al., 2016	Invalid assessment of fatigue
Backus et al., 2013	Abstract only
Cools et al., 2002	Invalid assessment of fatigue
Dube & Roy, 2019	Invalid assessment of fatigue
Ebaugh et al., 2006	Invalid assessment of fatigue
Gaudet et al., 2018	Invalid assessment of fatigue
Hammar skjöld & Harms-Ringdahl, 1992	Invalid assessment of fatigue
Hawkes et al., 2018	Invalid assessment of fatigue
Jensen et al., 2000	Invalid assessment of fatigue
Julienne et al., 2012	Invalid assessment of fatigue
Kawczyński et al., 2007	Invalid assessment of fatigue
Matthews et al., 2017	Invalid assessment of fatigue
McQuade et al., 1998	Invalid assessment of fatigue
Mullaney et al., 2006	Invalid assessment of fatigue
Niederbracht & Shim, 2008	Not intervention
Otto et al., 2018	Not comparator and inappropriate statistical comparison
Park et al., 2010	Not language
Pedersen et al., 1999	Invalid assessment of fatigue
Pontaga, 2018	Invalid assessment of fatigue
Spargoli, 2007	Not comparator and inappropriate statistical comparison
Suzuki et al., 2023	Invalid assessment of fatigue
Tse et al., 2016	Invalid assessment of fatigue
Umehara et al., 2018	Invalid assessment of fatigue
Weerakkody & Allen, 2017	Invalid assessment of fatigue
Yassierli & Nussbaum, 2007	Invalid assessment of fatigue